

#### US009318524B2

# (12) United States Patent

## Chappo et al.

#### (54) IMAGING DETECTOR WITH PER PIXEL ANALOG CHANNEL WELL ISOLATION WITH DECOUPLING

(71) Applicant: KONINKLIJKE PHILIPS N.V.,

Eindhoven (NL)

(72) Inventors: Marc Anthony Chappo, Elyria, OH

(US); Randall Peter Luhta, Chardon, OH (US); Chris J. Vrettos, Willoughby,

OH (US)

(73) Assignee: KONINKLIJKE PHILIPS N.V.,

Eindhoven (NL)

(\*) Notice: Subject to any disclaimer, the term of this

patent is extended or adjusted under 35

U.S.C. 154(b) by 0 days.

(21) Appl. No.: 14/390,809

(22) PCT Filed: Apr. 11, 2013

(86) PCT No.: **PCT/IB2013/052883** 

§ 371 (c)(1),

(2) Date: Oct. 6, 2014

(87) PCT Pub. No.: WO2013/164717

PCT Pub. Date: Nov. 7, 2013

(65) Prior Publication Data

US 2015/0090887 A1 Apr. 2, 2015

### Related U.S. Application Data

- (60) Provisional application No. 61/640,032, filed on Apr. 30, 2012.
- (51) **Int. Cl.** *H01L 27/146* (2006.01)

(10) Patent No.: US 9,318,524 B2

(45) **Date of Patent:** Apr. 19, 2016

(52) **U.S. CI.** CPC ..... *H01L 27/14634* (2013.01); *H01L 27/1463* 

(2013.01); **H01L** 27/1464 (2013.01); **H01L** 27/14661 (2013.01); **H01L** 27/14663 (2013.01)

(58) Field of Classification Search

CPC .... A61B 6/00; G01T 1/247; H01L 27/14634;

H01L 27/14663

See application file for complete search history.

#### (56) References Cited

#### U.S. PATENT DOCUMENTS

6,246,743	B1	6/2001	Kopp, III et al.
6,510,195	B1	1/2003	Chappo et al.
6,762,473		7/2004	Goushcha et al.
2006/0291115	A1*	12/2006	Song et al 361/56
2007/0045679	A1	3/2007	McKee et al.
2007/0246788	A1	10/2007	Mauritzson et al.
2009/0121146	A1	5/2009	Luhta et al.
2009/0314947	A1	12/2009	Goushcha et al.
2010/0108893	A1*	5/2010	Flitsch et al 250/361 R
2011/0155893	A1	6/2011	Endo et al.
2011/0221009	A1*	9/2011	Chuang et al 257/392
2012/0008031	A1	1/2012	Yamashita et al.

#### FOREIGN PATENT DOCUMENTS

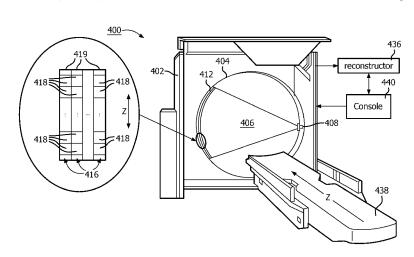
WO 2011126434 A1 10/2011 WO 2012001939 A1 1/2012

\* cited by examiner

Primary Examiner — Marcus Taningco (57) ABSTRACT

An imaging apparatus (400) includes a detector array (412) with at least one detector tile (418). The detector tile includes a photosensor array (422) with a two dimensional array of individual photosensitive detector pixels (424) located within a non-photosensitive area (426) and readout electronics (432) coupled to the photosensor array. The readout electronics includes individual analog readout channel wells (602, 604) corresponding to the individual detector pixels, wherein an analog readout channel well electrically isolates analog electrical components therein from analog electrical components in other analog readout channel wells. Decoupling circuitry optionally is located in at least one of metal layers of the individual analog readout channels or in the individual analog readout channel wells.

#### 18 Claims, 7 Drawing Sheets



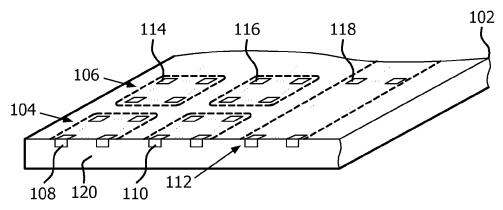


FIG. 1 Prior Art

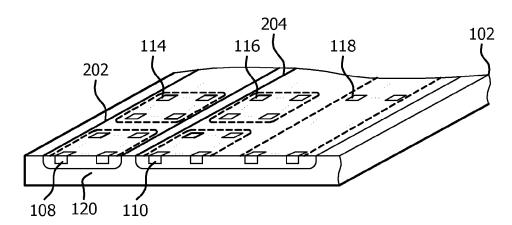


FIG. 2 Prior Art

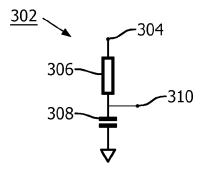
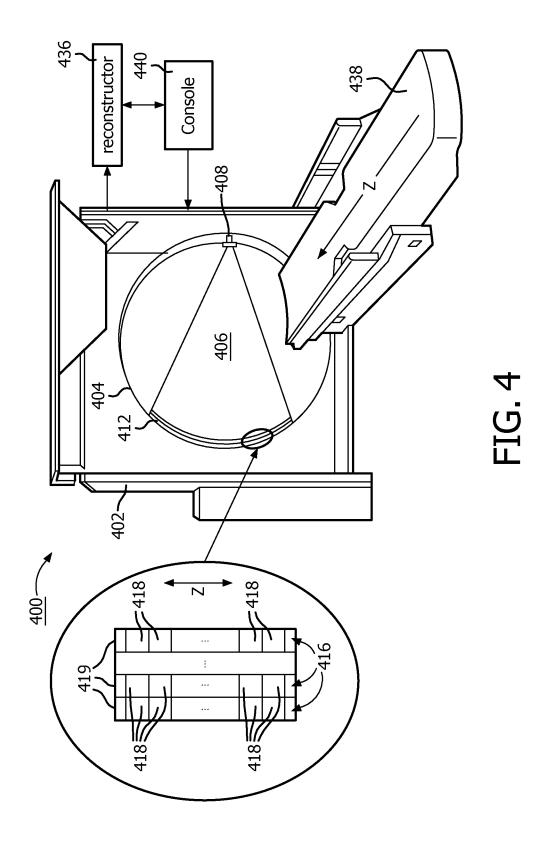


FIG. 3 Prior Art



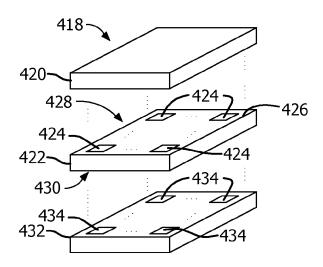


FIG. 5

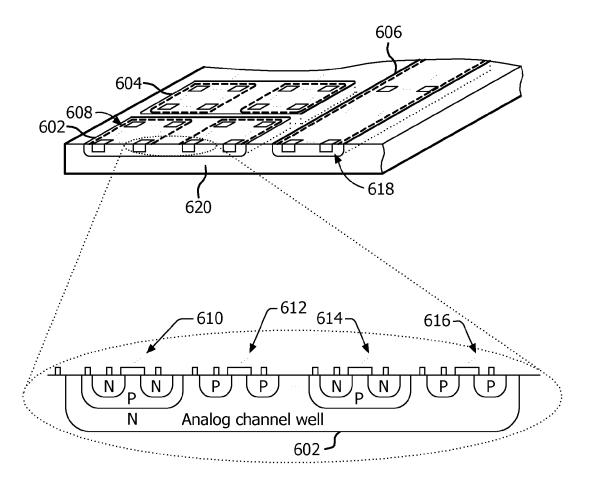


FIG. 6

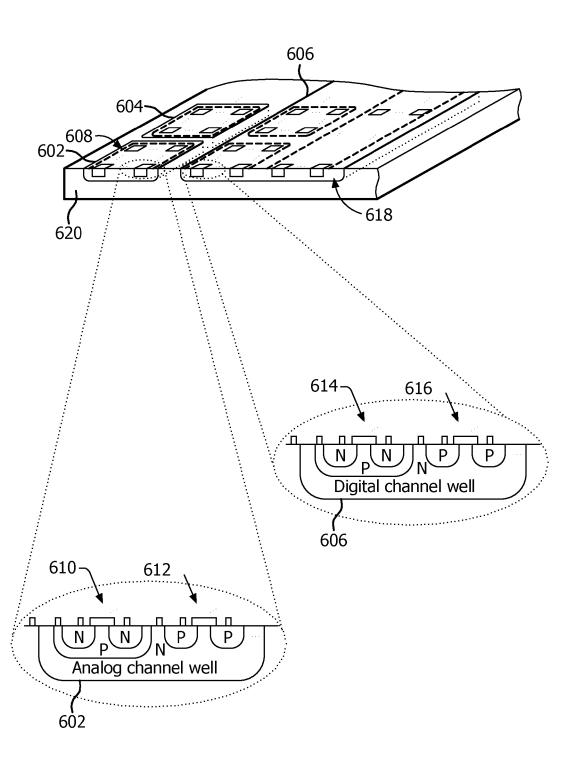


FIG. 7

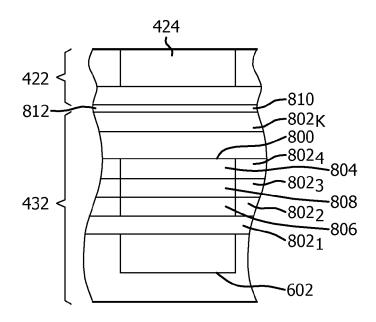


FIG. 8

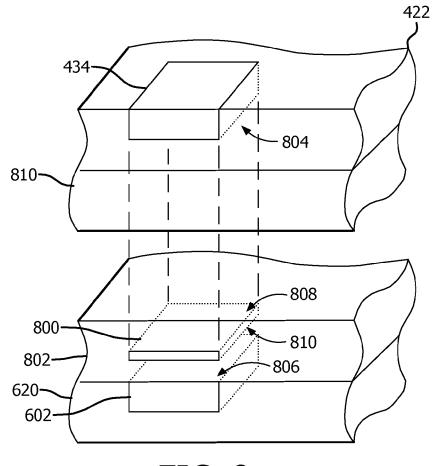


FIG. 9

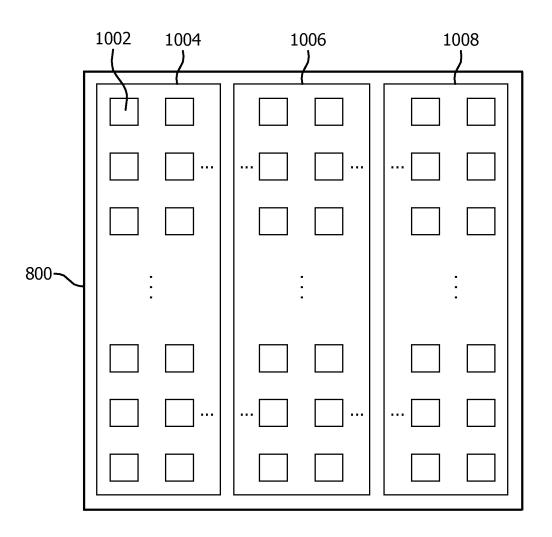


FIG. 10

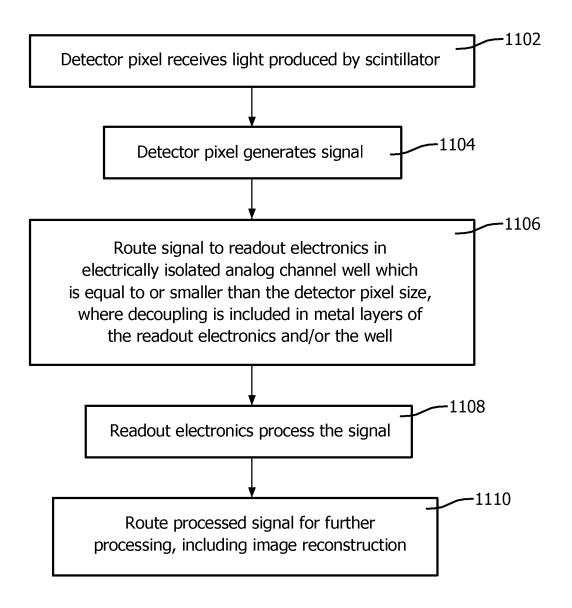


FIG. 11

#### IMAGING DETECTOR WITH PER PIXEL ANALOG CHANNEL WELL ISOLATION WITH DECOUPLING

## CROSS REFERENCE TO RELATED APPLICATIONS

This application is a national filing of PCT application Ser. No. PCT/1B2013/052833, filed Apr. 11, 2013, published as WO 2013/164717 A1on Nov. 7, 2013, which claims the benefit of U.S. provisional application Ser. No. 61/640,032 filed Apr. 30, 2012, which is incorporated herein by reference.

The following generally relates to an imaging detector and more particularly to an imaging detector with per pixel analog channel well isolation with decoupling and is described in 15 connection with computed tomography (CT).

A CT scanner generally includes an x-ray tube mounted on a rotatable gantry that rotates around an examination region about a z-axis. The x-ray tube emits radiation that traverses the examination region. A detector array subtends an angular 20 arc opposite the examination region from the x-ray tube, detects radiation that traverses the examination region, and generates a signal indicative thereof. A reconstructor processes the signal and reconstructs volumetric image data indicative thereof the examination region and a portion of a 25 subject or object located therein during scanning

The CT detector array described in U.S. Pat. No. 6,510,195 to Chappo et al. includes one or more rows of detector tiles. Each detector tile includes a scintillator layer optically coupled to a two-dimensional (2D) back-illuminated photodiode array of detector pixels (e.g., 16 or more). The photodiode array is bonded on a carrier substrate via bump bonding. Readout electronics packaged in an application specific integrated chip (ASIC) are also bonded on the carrier substrate. The carrier substrate includes electrodes that route signals 35 produced by the detector pixels to the readout electronics.

In U.S. patent application publication 2009/0121146 to Luhta et al., the CT detector tile includes a silicon photodiode with a photosensitive area and a non-photosensitive area. With this tile, the photodiode array is part of a photosensitive 40 area of the silicon substrate, and the non-photosensitive area includes electrodes that inter-connect each detector pixel to bonding pads. A silicon ASIC is directly bonded to the nonphotosensitive area of the silicon substrate in electrical communication with the bonding pads and hence the detector 45 pixels. The ASIC includes readout electronics for each detector pixel, including analog and digital electronics for each detector pixel. FIG. 1 shows a portion of an example prior art ASIC 102, which includes first readout electronics 104 for a first detector pixel and second readout electronics 106 for a 50 second different pixel. The first readout electronics 104 includes first analog components 108 and first digital components 110, and the second readout electronics 106 includes second analog components 114 and second digital components 116. The ASIC 102 also includes common digital elec- 55 tronics 112 including common digital components 118.

Note that the dashed lines around the components 108-118 do not indicate physical structure of the ASIC 102 but are included to clarify the illustrated groupings of the readout electronics components between analog, digital and common 60 digital and between pixels. Unfortunately, the analog and digital readout electronics 108-118 are in a same substrate 120 and are therefore susceptible to substrate noise. In addition, the analog and digital readout electronics 110-118 are in the same substrate 120 and therefore the analog readout electronics 108 and 114 are susceptible to noise from the digital readout electronics 110, 116 and 118 and vice versa.

2

One approach to mitigating noise contamination is to electrically isolate the analog and digital readout electronics and from the substrate and each other. This has been done through CMOS triple-well or shallow trench isolation, as shown in FIG. 2. In FIG. 2, a first well 202 electrically isolates the analog readout electronics 108 and 114 from the substrate 120 and the digital readout electronics 110, 116 and 118, and a second well 204 electrically isolates the digital readout electronics 110, 116 and 118 from the substrate 120 and the analog channels 108 and 114. However, this approach does not mitigate crosstalk between the readout electronics in a same well and such crosstalk can negatively affect detector linearity, gain, and noise performance, and limit low-dose imaging.

Decoupling circuitry has been used to decouple external power supplies and the power supplies of the readout electronic of the ASIC 102. For example, for the first readout electronics 104, separate decoupling circuitry is used for the analog, digital and common digital readout electronics 108, 110, and 112. FIG. 3 shows example decoupling circuitry 302 and includes an external power supply terminal 304, an RC filter resistor 306, an RC filter by-pass capacitor 308, and an internal readout electronics power supply terminal 310. Unfortunately, such circuitry includes electrical elements outside of the ASIC 102, which increases the overall footprint and cost of the detector, and adds unwanted inductance in series with resistor due to the interconnection distance from the circuit to the external substrate.

In view of at least the above, there is unresolved need for other readout channel and/or other decoupling configurations

Aspects described herein address the above-referenced problems and/or others.

In one aspect, an imaging apparatus includes a detector array with at least one detector tile. The detector tile includes a photosensor array with a two dimensional array of individual photosensitive detector pixels located within a non-photosensitive area and readout electronics coupled to the photosensor array. The readout electronics includes individual analog readout channel wells corresponding to the individual detector pixels, wherein an analog readout channel well electrically isolates analog electrical components therein from analog electrical components in other analog readout channel wells.

In another aspect, a method includes routing a detector pixel output signal to readout electronics corresponding only to the detector pixel, wherein the detector pixel is one of a plurality of detector pixels of an imaging detector, and wherein analog readout electronics of the readout electronics of the detector pixel are electrically isolated from analog readout electronics of other detector pixels through corresponding analog channel wells, and processing the signal with the readout electronics.

In another aspect, an imaging detector array includes a photosensor array with a two dimensional array of individual photosensitive detector pixels located within a non-photosensitive area. The imaging detector array further includes readout electronics coupled to the photosensor array, the readout electronics comprising: individual analog readout channel wells, each well including analog readout channel electronics and corresponding to an individual detector pixel, wherein the analog readout channel electronics in the individual analog readout channel wells are electrically isolated from each other. The imaging detector array further includes decoupling circuitry in metal layers of the individual analog readout channels.

The invention may take form in various components and arrangements of components, and in various steps and arrangements of steps. The drawings are only for purposes of illustrating the preferred embodiments and are not to be construed as limiting the invention.

FIG. 1 depicts a portion of a prior art imaging detector ASIC without electrical isolation between analog and digital readout electronics and the substrate.

FIG. 2 depicts a portion of a prior art imaging detector ASIC in which analog and digital readout electronics are 10 electrically isolated from each other and the substrate through a common analog well and a common digital well.

FIG. 3 depicts prior art external decoupling circuitry for the readout electronics of FIG. 1 or 2.

FIG. 4 illustrates an imaging system including a detector 15 tile with at least analog readout electronics electrically isolated on a per pixel basis and including decoupling in the ASIC.

FIG. 5 schematically illustrates an example of the detector tile

FIG. 6 schematically illustrates an example of the detector tile in which analog and digital readout electronics for each detector pixel are located in a corresponding analog channel well.

FIG. 7 schematically illustrates a variation of FIG. 6 in 25 which the analog and the digital readout electronics of a pixel are located in different wells.

FIG. 8 schematically illustrates an example detector tile in which decoupling circuitry is located in the layers of the readout electronics.

FIG. 9 illustrates a perspective view of the detector tile of FIG. 8, showing the geometrical relationship between the decoupling circuitry and an individual well.

FIG. 10 illustrates an example configuration of the decoupling capacitor.

FIG. 11 illustrates an example method.

In initially referring to FIG. 4, an imaging system 400, such as a computed tomography (CT) scanner, is illustrated. The imaging system 400 includes a generally stationary gantry 402 and a rotating gantry 404. The rotating gantry 404 is 40 rotatably supported by the stationary gantry 402 and rotates around an examination region 406 about a longitudinal or z-axis. A radiation source 408, such as an x-ray tube, is supported by and rotates with the rotating gantry 404, and produces a generally cone, fan, wedge, or otherwise shaped 45 radiation beam that traverses the examination region 406.

A radiation sensitive detector array 412 subtends an angular arc opposite the radiation sources 408 across the examination region 406 and detects radiation traversing the examination region 406. The radiation sensitive detector array 412 includes one or more rows 416 of detector tiles 418, the rows 416 arranged with respect to each other along the z-axis. The detector tiles 418 are coupled to detector modules 419, via solder balls, stud bumps, and/or otherwise, which are mounted in the system 400, arranged with respect to each 55 other along the z-axis. Briefly turning to FIG. 5, a non-limiting example of a detector tile 418 is illustrated. For clarity and explanatory purposes, the tile 418 is shown in an exploded view in which various components thereof are separated from each other.

The tile 418 includes a scintillator layer 420 optically coupled to a photosensor 422, which includes a plurality of photosensitive areas (detector pixels) 424 within a non-photosensitive area 426 on a first side 428 of the photosensor 422. The illustrated photosensor 422 is a back-illuminated photosensor with electrodes (not visible) that inter-connect the detector pixels 424 to bonding pads or the like (not visible)

4

located on a second opposing side 430 of the photosensor 422. In another embodiment, the photosensor 422 is a front-illuminated photosensor with vias that route the signals from the first side 428 to the pads on the opposing side 430. The scintillator layer 420 may include a plurality of scintillator pixels, each corresponding to one of the detector pixels 424.

An ASIC (readout electronics) 432 includes a plurality of pixel channel wells 434. Each channel well 434 corresponds to only one of the detector pixels 424. A channel well 434 includes one or more electrical components, such as transistors and/or other electronics, for its corresponding detector pixel 424. The illustrated ASIC 432 has a one to one geometric relationship with the photosensor 422, and each channel well 434 has a one to one geometric relationship with a detector pixel 424. That is, surfaces of the ASIC 432 and the photosensor 422 that are bonded are approximately a same size. Likewise, surfaces of a well 434 and detector pixel 424 are approximately the same size. In another embodiment, the surfaces are not the same size, for example, the ASIC 432 is smaller than the photosensor 422.

As described in greater detail below, an individual channel well 434 electrically isolates at least the analog electrical components of a channel from the analog electrical components of the other channels. Isolating the analog electrical components as such mitigates crosstalk between the analog electrical components of the different channels of the different detector pixels 424. This may improve detector linearity, gain, and noise performance, relative to a configuration in which the wells 434 are omitted. This also renders the system 400 well-suited for low-dose imaging. Also described in greater detail below, the ASIC 432 includes decoupling circuitry for each channel contained in a well 434 in metal layers of the ASIC 432. As such, decoupling can be provided at the ASIC level, without requiring additional space.

The ASIC 432 and the photosensor 422 are bonded together with the ASIC channels 434 in electrical communication with the bonding pads of the photosensor 422. In the illustrated embodiment, both the photosensor 422 and the ASIC 432 include silicon and are bonded together via glue, solder ball, flip chip, covalent bonding, and/or other siliconto-silicon bonding approaches. An example of semiconductor silicon-to-silicon bonding is discussed in U.S. patent application publication 2009/0121146 to Luhta et al., which is incorporated herein by reference in its entirety. Optionally, an interposer substrate may be placed between the assemblies 422 and 432 with pass-through connections to facilitate assembly at some additional cost.

Returning to FIG. 4, a reconstructor 436 reconstructs the signal from the detector array 412, generating volumetric three-dimensional image data. A support 438, such as a couch, supports the object or subject in the examination region 406. A general purpose computing system serves as an operator console 440, which includes human readable output devices such as a display and/or printer and input devices such as a keyboard and/or mouse. Software resident on the console 440 allows the operator to control the operation of the imaging system 400

FIG. 6 shows a portion of the ASIC 432. In this example, the ASIC 432 includes at least one analog pixel channel well 60 602, 604, . . . , and at least one digital common well 606. The ASIC 432 may also include at least one analog common well and/or one or more other wells.

The at least one analog pixel channel well **602** includes a plurality of channels **608**, each including an analog N-channel field-effect transistor (NFET) **610**, an analog P-type field-effect transistor (PFET) **612**, a digital NFET **614**, and a digital PFET **616** in an N-type analog channel well. P-type wells and

corresponding transistor configurations are also contemplated herein. The at least one common digital well **606** also includes a plurality of channels **618**, such as NFETs and PFETs. Likewise, the common digital well **606** may alternatively include a P-type well.

For any given analog pixel channel well, for example, the well 602, the transistors (610-616) therein are electrically isolated from the transistors of another analog channel well, for example, the analog channel well 604. The channel wells 602, 604 and 606 also electrically isolate the transistors therein from a substrate 620, in which the wells 602, 604 and 606 are located. The isolation of circuitry in wells 602, 604 and 606 can be formed via triple-well isolation and/or other approaches such as STI (Shallow Trench Isolation) for providing isolation in silicon semiconductor material.

FIG. 7 shows a variation of the portion of the ASIC 432 in which the digital transistor 614 and 616 are located in the digital common well 606 instead of in the analog channel well 602. In this embodiment, the analog transistors 610 and 612 are still located in the analog channel well 602 but the digital 20 transistors 614 and 616 are located in the digital channel well 606. This configuration additionally electrically isolates the analog transistors 610 and 612 and the digital transistors 614 and 616 of a detector pixel.

The configurations shown in FIGS. **6** and **7** at least provide 25 analog channel to analog channel electrical isolation between detector pixels by electrically isolating the analog transistors of the analog channel of one detector pixel from the analog transistors of other analog channels of another detector pixel via analog channels wells (e.g., wells **602** and **604**). Such a 30 configuration confines channel activity to a single well, mitigating channel-to-channel crosstalk.

It is to be appreciated that this can improve detector linearity and noise performance relative to a configuration in which the individual channels are not electrically isolated from each 35 other, for example, those shown in connection with FIG. 1 and/or 2. As shown in FIG. 7, the analog and digital transistors of a channel can also be electrically isolated by separating them into different wells, which mitigates analog and digital noise contamination for a single channel.

FIG. 8 schematically illustrates an embodiment in which the ASIC 432 includes a decoupling capacitor 800 for each detector pixel of the detector pixels 424. For clarity and sake of brevity, only one decoupling capacitor 800 is shown in connection with a corresponding detector pixel 424 and analog ASIC well 602. However, it is to be understood that the decoupling capacitors 800 for other detector pixels 424 and wells 602 are similar.

The ASIC 432 includes a plurality of metal layers 802, including layers  $802_1$ ,  $802_2$ ,  $802_3$ ,  $802_4$ , ...,  $802_K$  (where K 50 is an integer greater than one). The photosensor 422 may or may not include a plurality of metal layers 810. In the illustrated embodiment, the photosensor layers 810 are coupled via to the ASIC 802 of the ASIC 432 such that the detector pixel 424 is in electrical communication with the readout 55 electronics of the well 602. The electrical connections are not shown for sake of clarity.

In FIG. 8, the decoupling capacitor 800 includes a first electrode 804 in the layer 802<sub>4</sub>, a second electrode 806 in the layer 802<sub>2</sub>, an insulating layer 808 disposed there between 60 (and in the layer 802<sub>3</sub>) and including a dielectric material with a predetermined dielectric constant, forming a capacitor structure in the layers 802. Metal-insulator-metal (MIM) and/or other fabrication processes can be used to fabricate the decoupling capacitor 800.

FIG. 9 shows a perspective view of the embodiment of FIG. 8, showing an example geometrical relationship between the

6

detector pixel 424, the decoupling capacitor 800, and the channel well 602. In this embodiment, there is a one to one geometrical relationship between an area 804 of the detector pixel 424 facing an area 804 of the detector well 602 and a one to one geometrical relationship between an area 804 of the detector pixel 424 facing an area 808 of the decoupling capacitor 800, and hence, a one to one geometrical relationship between an area 810 of the decoupling capacitor 800 facing an area 804 of the well 602. Non one to one relationships are also contemplated herein.

FIG. 10 shows an example configuration of the decoupling capacitor 800, which includes a plurality of sub-capacitors 1002. In this example, a first grouping 1004 of sub-capacitors are electrically connected in parallel to form a decoupling capacitor for the positive power supply of the analog readout electronics, a second grouping 1006 of sub-capacitors are electrically connected in parallel to form a decoupling capacitor for the power supply of the analog readout electronics, and a third grouping 1008 of sub-capacitors are electrically connected in parallel to form a decoupling capacitor for digital readout electronics. The grouping 1004, 1006 and 1008 may or may not have a same capacitance, but the capacitance of each grouping will be suitable to form reasonable decoupling capacitors.

FIG. 11 illustrates a method.

At 1102, a detector pixel of a photosensor array receives light produced by a scintillator in response to detection of x-ray radiation.

At 1104, the detector pixel generates a signal indicative of the received light.

At 1106, the signal is routed to readout electronics corresponding to the detector pixel, wherein at least analog components of the readout electronics are electrically isolated from analog components of readout electronics of other detector pixels via individual channel wells (which are equal to or smaller than the detector pixel size), with decoupling in metal layers of the readout electronics.

At 1108, the readout electronics processes the signal.

At 1110, the processed signal is routed from the readout electronics to another component for further processing, including reconstruction.

It is to be appreciated that the ordering of the acts in the methods described herein is not limiting. As such, other orderings are contemplated herein. In addition, one or more acts may be omitted and/or one or more additional acts may be included.

The invention has been described with reference to the preferred embodiments. Modifications and alterations may occur to others upon reading and understanding the preceding detailed description. It is intended that the invention be constructed as including all such modifications and alterations insofar as they come within the scope of the appended claims or the equivalents thereof.

The invention claimed is:

- 1. An imaging apparatus, comprising:
- a detector array with at least one detector tile, the detector tile, comprising:
  - a photosensor array with a two dimensional array of individual photosensitive detector pixels located within a non-photosensitive area; and
  - readout electronics coupled to the photosensor array, the readout electronics comprising:
    - individual analog readout channel wells corresponding to the individual detector pixels, wherein an analog readout channel well electrically isolates

7

analog electrical components therein from analog electrical components in other analog readout channel wells;

a plurality of metal layers; and

decoupling capacitors for analog and digital circuitry 5 of at least one detector pixel, wherein the decoupling capacitors are located in the plurality of layers between the detector pixel and the analog readout channel well corresponding to the detector pixel.

- 2. The imaging apparatus of claim 1, further comprising: at least one analog transistor for a detector pixel; and
- at least one digital transistor for the same detector pixel, wherein the at least one analog transistor and the at least one digital transistor for the same detector pixel are 15 located in a same analog readout channel well for the same detector pixel.
- 3. The imaging apparatus of claim 1, further comprising: a common digital readout channel well, which includes readout electronics common to the individual detector 20 located in a common digital channel well.

at least one analog transistor for a detector pixel; and

- at least one digital transistor for the same detector pixel,
- wherein the at least one analog transistor is located in the analog readout channel well for the detector pixel and the at least one digital transistor is located in the common digital readout channel well.
- 4. The imaging apparatus of claim 1, wherein the photosensor array is a silicon photosensor array and the readout electronics are part of a silicon integrated circuit, and the 30 silicon integrated circuit and the photosensor array are bounded via silicon-to-silicon bonding.
- 5. The imaging apparatus of claim 1, wherein a decoupling capacitor includes two conductive electrodes located in two different layers and an insulator located in a third layer, which 35 is located between the two different layers.
- 6. The imaging apparatus of claim 1, wherein a geometry of the decoupling capacitors in aggregate is approximately equal to a geometry of the analog readout channel well.
- 7. The imaging apparatus of claim 1, wherein a geometry of 40 the readout electronics is equal to or smaller than a geometry of the photosensor array.
- 8. The imaging apparatus of claim 1, wherein the photosensor array includes back-illuminated photodiodes or frontilluminated photodiodes.
- 9. The imaging apparatus of claim 1, wherein the readout electronics and the photosensor array include silicon substrates bonded together through a silicon-on-silicon bond.
  - 10. A method, comprising:

routing a detector pixel output signal to readout electronics 50 corresponding only to the detector pixel, wherein the

detector pixel is one of a plurality of detector pixels of an imaging detector, and wherein analog readout electronics of the readout electronics of the detector pixel are electrically isolated from analog readout electronics of the readout electronics of other detector pixels through corresponding analog channel wells:

decoupling the analog and digital readout electronics from corresponding power supplies using a decoupling capacitor and

processing the signal with the readout electronics.

- 11. The method of claim 10, wherein the decoupling capacitor includes three distinct regions, two for the analog readout electronics and one for the digital readout electronics.
- 12. The method of claim 10, wherein digital readout electronics of the readout electronics of the detector pixel are located in the corresponding analog channel well.
- 13. The method of claim 10, wherein digital readout electronics of the readout electronics of the detector pixel are
  - **14**. An imaging detector array, comprising:
  - a photosensor array with a two dimensional array of individual photosensitive detector pixels located within a non-photosensitive area;
  - readout electronics coupled to the photosensor array, the readout electronics comprising: individual analog readout channel wells, each well including analog readout channel electronics and corresponding to an individual detector pixel, wherein the analog readout channel electronics in the individual analog readout channel wells are electrically isolated from each other; and

decoupling circuitry in metal layers of the individual analog readout channels.

- 15. The imaging detector array of claim 14, the readout electronics for each pixel further comprising: digital readout electronics, wherein the digital readout electronics are located in the corresponding analog channel well.
- 16. The imaging detector array of claim 14, the readout further comprising: a common digital channel well, and the readout electronics for each pixel further comprising: digital readout electronics, wherein the digital readout electronics are located in the common digital channel well.
- 17. The imaging detector array of claim 14, wherein a geometry of a well is approximately equal to a geometry of the corresponding detector pixel.
- 18. The imaging detector array of claim 14, wherein a geometry of the decoupling capacitor for an analog channel well is approximately equal to a geometry of the corresponding detector pixel.